

Characterization of filter materials for single-shot dual-energy imaging

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1. Introduction

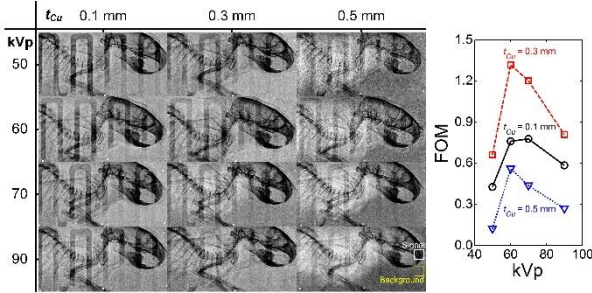


Fig. 1. Bone-enhanced DE images obtained for a postmortem mouse using the sandwich detector for various combinations of kVp and t_{Cu} .

We previously described the sandwich configuration detector by stacking two flat-panel detectors (FPDs) and demonstrated its prospect for “motion-artifact-free” single-shot dual-energy (DE) imaging by obtaining bone and soft-tissues images of a postmortem mouse [1, 2]. The two FPDs used the same CMOS photodiode arrays but the scintillators with different thicknesses: the thicker one for the rear FPD to achieve high quantum efficiency with the higher-energy x-ray spectrum. An intermediate copper filter was used to further increase energy separation between the two FPDs. According to another previous study, bone-enhanced DE images were obtained for a postmortem mouse using the sandwich detector for various combinations of kVp and t_{Cu} . The DE images were obtained by using weighted logarithmic subtraction of two images obtained from the front- and rear- detector. For the maxillary bone and neighboring background regions, the figure of merits (FOM) were calculated using Eq. 1, and the results are shown in figure 1.

2. Materials and Methods

2.1 Sandwich detector

The sandwich detector consisted of FPDs and intermediate filter for various materials and thickness. The FPDs used the same photodiode array (RadEye1TM, Teledyne Rad-ikon Imaging Corp., Sunnyvale, CA) and gadolinium oxysulfide (Gd₂O₂S : Tb) phosphor screens (Carestream Health Inc., Rochester, NY) with different thickness: thinner (~ 34 mg cm⁻²) for the front and thicker (~ 67 mg cm⁻²) for the rear detector layers, respectively. The photodiode array had 0.048 mm-sized pixels arranged in 512 × 1024 format.

2.2 Fourier performance

The detective quantum efficiency (DQE) of the j th detector layer (j designates F or R for front or rear detector, respectively) is given by

$$DQE_j(u) = \frac{\bar{q}_{in} G_j^2 MTF_j^2(u)}{NPS_j(u)} = \frac{MTF_j^2}{\bar{q}_{in} [NPS_j(u)/\bar{d}_j^2]}$$

where \bar{q} (mm²) denotes the average incident photon fluence. G (DN mm²) is the detector gain relating \bar{q} to the average pixel signal \bar{d} in units of digital number (DN).

We measure the modulation-transfer function (MTF), noise-power spectrum (NPS), and DQE of each detector layer of the sandwich detector for various tube voltages, materials and thicknesses of an intermediate filter.

2.3 Cascaded-system analysis

In a previous study, we showed the cascaded model describing the signal and noise from each detector layer in the sandwich detector [6]. Similar to Fourier performance, we can describe the DQE of the j th detector layer of the sandwich detector in cascaded-system analysis model as follows:

$$DQE_j(u) = \frac{MTF_j^2(u)}{\bar{q}_{in} [W'_{j,indirect}(u) + W'_{j,direct}(u) + W'_{j,add}(u)]}$$

To investigate spectral energy separation for various filter materials in the sandwich detector. We may construct the FOM in the single-shot DE images using Eq 4.

$$FOM_j = C_j^2 A_{eff} \bar{q}_0 \left[\frac{\omega_j^2}{DQE^F(0)} + \frac{1}{DQE^R(0)} \right]^{-1}$$

3. Preliminary results

Figure 2(a) shows incident x-ray spectra for rear in the sandwich detector after transmitted the front detector and various filter materials. The spectra transmitted through the various filter materials all have a transmittance of $\sim 30\%$. Then, filter thickness are Cu = ~ 0.18 mm, Mo = ~ 0.06 mm, Gd = ~ 0.13 mm, Sn = ~ 0.07 mm, respectively.

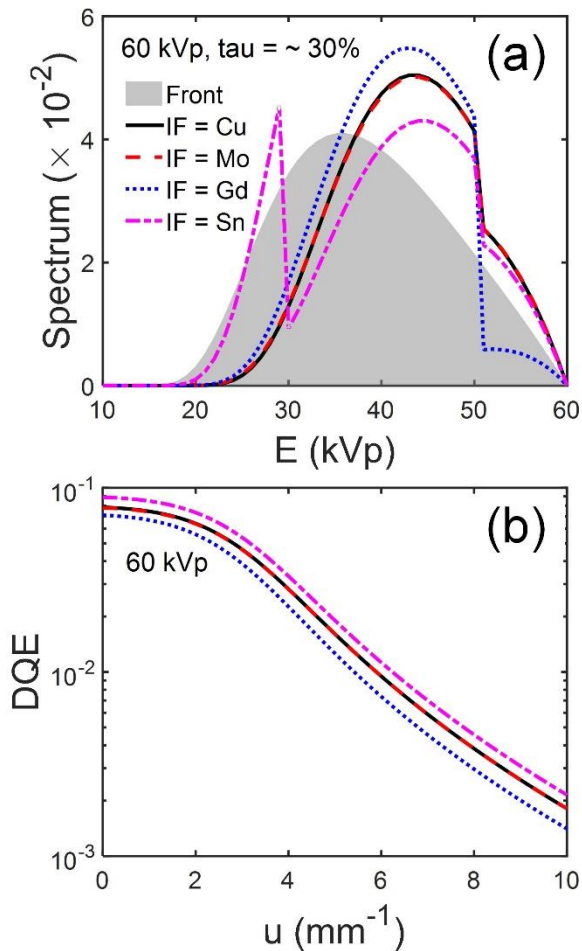


Fig. 2. (a) Spectra after transmission front detector and various intermediate filter with $\tau = \sim 30\%$. (b) Spatial-frequency-dependent DQE with 60 kVp, ~ 20 mR.

Figure 2(b) is spatial-frequency-dependent DQE of the rear detector layer at 60 kVp, ~ 20 mR with filter materials.

4. Further study

The remained further study before the meeting includes the followings:

- the quantitative analysis of the measured MTF, NPS, and DQE characteristics for various intermediate filter with the helps from the developed model or simulations;
- the quantitative analysis of the correlated or K-fluorescence x-ray generated from various filter materials;
- quantitatively analysis of the single-shot dual-energy imaging for various filter materials;

Acknowledgments

This work was supported by the National Research Foundation of Korea (NRF) grant funded by the Korean government (MSIP) (No. 2017M2A2A6A01019930).

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